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## 8 **Exhaled breath gas sensing using pristine and functionalised** 9 **WO<sub>3</sub> nanowire sensors enhanced by UV-light irradiation**

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## 22 **Abstract**

23 The development of advanced metal-oxide-semiconductor (MOS) sensing technologies for the  
24 detection of volatile organic compounds (VOCs) present in the exhaled breath is of great  
25 importance for non-invasive, cheap and fast medical diagnostics. Our experimental studies  
26 investigate the effects of operating temperature selection and UV-light irradiation on improving  
27 the sensitivity of WO<sub>3</sub> nanowire sensors for exhaled breath exposure. Herein, six WO<sub>3</sub> nanowire  
28 sensors (both pristine and doped with a range of metal nanoparticles such as Pt, Au, Au/Pt, Ni  
29 and Fe) were synthesised via aerosol-assisted chemical vapour deposition (AACVD) and  
30 characterised by means of atomic force microscopy (AFM), scanning electron microscopy  
31 (SEM), transmission electron microscopy (TEM) and energy dispersive X-ray (EDX-ray).  
32 Breath measurements were performed in the dark and under UV-light irradiation at various  
33 sensor operating temperatures. The results demonstrate that UV-light irradiation combined with  
34 the optimisation of the sensors' operating temperature can greatly enhance the sensors'  
35 responses towards breath exposure.



## 36 **Keywords**

37 WO<sub>3</sub> nanowire sensors, metal nanoparticles, sensitivity enhancement, UV-light irradiation,  
38 operating temperature, exhaled breath analysis.

## 39 **1. Introduction**

40 Exhaled breath is a valuable, non-invasive biological tool available for diagnosing and  
41 monitoring medical conditions (Gardner et al., 2000; Adiguzel & Kulah 2015;  
42 Lentka et al., 2016; Saidi et al., 2018). Its popularity in medicine can be demonstrated by an  
43 increase in papers published in this area. Therefore, the development of advanced and cheap  
44 sensors of high sensitivity towards low concentrations of VOCs in the exhaled breath is of  
45 paramount importance. In this regard, MOS chemical gas sensors have emerged as a very  
46 promising tool for monitoring low concentrations of gaseous compounds  
47 (Konvalina & Haick 2014; Welearegay et al., 2016; Zhang et al., 2017), and they represent a  
48 low-cost alternative as compared to other available analytical methods  
49 (e.g., Gas Chromatography/Mass Spectrometry) that require expensive and bulky equipment.

50 Tungsten trioxide (WO<sub>3</sub>), with a band gap of about 2.8 eV (Yun et al., 2016), is one of the most  
51 important n-type MOSs, and it has been extensively used as a gas sensor material  
52 for VOC detection (Righettoni et al., 2010; Choi et al., 2014; Kim et al., 2016;  
53 Shendage et al., 2017). However, its selectivity and sensitivity are still too low for some  
54 applications, such as breath analysis. The selectivity can be partially improved by using a set  
55 of sensors with different cross-sensing performances and enhanced by reducing the particle size  
56 to a range of 5 to 50 nm (Yamazoe, 1991; Shimizu and Egashira, 1999; Ederth et al., 2006).  
57 Alternatively, the sensing potential of WO<sub>3</sub> sensors can be significantly improved by doping  
58 the sensing layer with a small amount of metal nanoparticles (NPs), such as platinum, gold,  
59 nickel, iron, etc. (Vallejos et al., 2013; Ahsan et al., 2013; Vilic and Llobet 2016). Metal doping



60 is considered a crucial option for diversifying the selectivity and improving the sensitivity of  
61 the sensors. Nevertheless, the sensing performance of the  $\text{WO}_3$  sensors must be further  
62 optimised to satisfy the requirements for breath analysis applications.

63  $\text{WO}_3$  NW sensors generally operate at elevated temperatures because the detection mechanisms  
64 are based on thermo-activated chemical reactions between the sensing film and the adsorbed  
65 VOCs (Bendahan et al., 2007). Variation of the sensor's operating temperature may enhance its  
66 sensitivity (Paulsson and Winqvist, 1999; Taurino et al., 2002; Ionescu and Llobet 2002;  
67 Zhang et al., 2015). Besides, many researchers have proven that  $\text{WO}_3$  sensor performance could  
68 be influenced by a photocatalytic effect such as UV-light irradiation (Iliev et al., 2010;  
69 Giberti et al., 2012; Smulko et al., 2015; Trawka et al., 2016; Gonzalez et al., 2016).  
70 The sensitive film of the sensor absorbs the UV-light (Mishra et al., 2004), which provides a  
71 further dissociation of the gaseous compounds and the consequent molecule adsorption  
72 (Trawka et al., 2016). UV-light irradiation creates a charge transport that increases the density  
73 of free electron-hole pairs (Karaduman et al., 2014; Xu et al., 2015). Therefore, it alters the  
74 sensing layer. Moreover, the applied UV-light of selected wavelengths can modulate the  
75 sensing properties in a different way due to various penetration depths, related to the applied  
76 wavelength and morphology of the porous gas sensing layer. Altogether, the response of MOS  
77 gas sensors can be successfully modified by UV-light that reduces the necessary heating energy  
78 (Park et al., 2013; Espid and Taghipour, 2017).

79 In our paper, pristine and metal-doped  $\text{WO}_3$  NWs were elaborated using aerosol-assisted  
80 chemical vapour deposition (AACVD) and characterised by using Atomic Force Microscopy  
81 (AFM), Scanning Electron Microscopy (SEM), Transmission Electron Microscopy (TEM) and  
82 Energy Dispersive X-ray (EDX-ray). The effects of UV-light irradiation and operating  
83 temperature selection were investigated regarding the analysis of exhaled breath.



## 84 2. Materials and methods

### 85 2.1. Sensor fabrication

86 AACVD was used to grow  $\text{WO}_3$  NWs due to its simplicity and relatively low temperature  
87 experimental conditions (Annanouch et al., 2013; Qadri et al., 2016). This method consists of  
88 delivering a suitable precursor in the form of an aerosol into the reactor where the substrate is  
89 mounted (Stoycheva et al. 2012).

90 In our study, six different sensors (*i.e.*, pristine  $\text{WO}_3$  NWs and the following pool of metal-  
91 doped  $\text{WO}_3$  NWs: Pt/ $\text{WO}_3$ ; Au/Pt/ $\text{WO}_3$ ; Au/ $\text{WO}_3$ ; Ni/ $\text{WO}_3$ ; and Fe/ $\text{WO}_3$ ) were grown using  
92 AACVD. Alumina substrates with Pt interdigitated electrodes on the front-side and  
93 a Pt meander heater on the back-side were employed as sensing substrates from *CeramTec*®  
94 (Marktredwitz, Germany). The substrates were successively cleaned with ethanol, acetone and  
95 distilled water and dried with a nitrogen flow before they were placed inside the AACVD  
96 reactor.

97 The layers of  $\text{WO}_3$  NWs were prepared using tungsten hexacarbonyl ( $\text{WC}_6\text{O}_6$ ) as a precursor  
98 according to previous reported procedures (Annanouch et al., 2015; Thamri et al., 2016). The  
99 experimental conditions for growing the six sensors are provided in Table 1. After nanomaterial  
100 synthesis, the deposited films were annealed in an oven (Carbolite's calcination furnace  
101 1200 °C | BWF) at 500 °C for 180 minutes under a constant flow of 200 mL/min of synthetic  
102 air. This step was carried out in order to clean the surface of deposition residues and to stabilise  
103 and crystallise the structure of the grown nanomaterials (Stankova et al., 2005; Ng et al., 2015).  
104 Otherwise, the morphology and composition of the deposited films were characterised.  
105 SEM measurements were performed using a FEI-ESEM Quanta 600 equipment (20 keV),  
106 which was coupled to an EDX analyser from *Oxford Instruments*. A TEM analysis of the  
107 Nanoparticles' sizes was done by JEOL JEM-1011 equipment with an accelerating energy of

108 100 keV while the structure of the deposited film was studied with AFM by means of a Keysight  
109 5500 SPM.

110 AACVD reaction of  $WC_6O_6$  with a mixture of acetone and methanol, inside a hot wall reactor,  
111 resulted in the formation of blue-black  $WO_3$  films. Applying the annealing process on these  
112 films at 500 °C yielded yellow layers that indicated fully oxidised  $WO_3$ . AFM analysis was used  
113 in acoustic mode to assess a topography of the annealed surface of the deposited layers. Figure  
114 1 presents orthogonal 3D images of the AFM topography of pristine and functionalised  $WO_3$   
115 films deposited onto alumina substrate which is scanned within an area of 10  $\mu m^2$ . It can be  
116 seen that the maximal heights of the pristine  $WO_3$  and Fe/ $WO_3$  NWs were 2.2  $\mu m$  and 3.4 nm,  
117 respectively (Fig. 1.a, Fig. 1.f). However, a significant reduction of surface roughness was  
118 achieved by functionalising the sensing surface with metal nanoparticles (except for Fe  
119 nanoparticles). Maximal heights of 762 nm, 713 nm, 991 nm and 505 nm for Pt/ $WO_3$  (Fig. 1.b),  
120 Au/Pt/ $WO_3$  (Fig. 1.c), Au/ $WO_3$  (Fig. 1.d) and Ni/ $WO_3$  (Fig. 1.e) were obtained, respectively. In  
121 all cases, AFM images showed complete coverage of the  $WO_3$  films on the entire substrate  
122 surface. It seems that the shape of the grains varied when changing the catalysts. Figure 2.a  
123 shows a typical SEM image of the pristine  $WO_3$ . It can be seen that the AACVD method  
124 at 500 °C produced a layer of thick NWs (about 159 nm), with high density and quite  
125 a homogeneous distribution on the entire substrate. In contrast, the films that contain Pt and/or  
126 Au Nps exhibited a mixture of randomly distributed nanowires with a diameter ranging between  
127 45 and 57 nm (Fig. 2.b, Fig. 2.c and Fig. 2.d). The layer of Ni/ $WO_3$  showed high density NWs  
128 which were randomly distributed (Fig. 3.e). SEM data of Fe/ $WO_3$  also show NWs of various  
129 sizes with a diameter ranging between 47 and 126 nm (Fig. 2.f). The AACVD yields a high  
130 density of non-aligned nanowires, with a relatively homogeneous distribution containing small  
131 pores over the studied surfaces. TEM of the deposited layers for pristine and functionalised  
132  $WO_3$  displayed porous polycrystalline films in thinner structures, approximately as spherical or

133 cylindrical morphologies (Fig. 3). Nanowires and nanoparticles can be easily observed from  
134 the recorded images. They appear well dispersed along the surface of the  $\text{WO}_3$  films. The grain  
135 diameters of the studied metal Nps were about 11 nm for Pt Nps (Fig. 3.b), 4.63 nm for the  
136 alloy of Au/Pt Nps (Fig. 3.c), 3.97 nm for Au Nps (Fig. 3.d), 39 nm for Ni Nps (Fig. 3.e) and  
137 8.22 nm for Fe Nps (Fig. 3.f). The results show that the set of the investigated sensors was  
138 characterised by their high surface-to-volume ratio, which provides more surface area for both  
139 chemical and physical interactions and therefore secures better sensitivity. The EDX spectrum  
140 (Fig. 4) showed tungsten, oxygen and alumina (from the substrate) as the major peaks, and also  
141 revealed the presence of metal nanoparticles on the surface of the sensing nanomaterials.  
142 The percentages of metal nanostructures on the sensing films varied between 1% and 2% except  
143 for Pt Nps where it is found within 6% to 7% due to presence of platinum connectors to  
144 the substrate.

## 145 **2.2. Measurement set-up and conditions**

146 The main part of the presented experimental studies required a collection of exhaled breath  
147 samples. To avoid any eventual artefacts, the breath samples were taken from the same  
148 individual (non-smoker, adult man) using Tedlar® bags before any food or beverage  
149 consumption. For this, the person took a deep breath, and breathed normally into the collection  
150 bag before emptying his lungs. The breath sample was immediately transferred from the  
151 collection bag into the gas chamber where the sensors were placed. This was done by pumping  
152 the contents of each filled bag at a constant flow rate of 100 mL/min.

153 The experiments began by starting a flow of current through the sensors' heaters, corresponding  
154 to the selected temperature, for 1000 s. Next, the sensors were exposed to the collected breath  
155 sample for 40 min, and ended with the next 80 min of recovery under laboratory air using the  
156 same flow rate of 100 mL/min. An exposure of the sensors' to the exhaled breath was done both  
157 in dark and under UV-light irradiation. The sensors' conductance was continuously recorded at

158 a sampling rate of 1 Hz using an NI USB-6212 data acquisition board from *National*  
159 *Instruments* (Texas, USA). The sensors' conductance was determined by measuring the DC  
160 voltage across the sensor as part of a voltage divider with another resistor connected in series  
161 and supplied by a DC voltage of 5 V. Figure 5 shows the circuit of the electrical current control  
162 unit for the heaters of three sensors. This unit was repeated to supply DC current for the next  
163 three heaters. The operating temperature was controlled by choosing the resistances of the  
164 heaters (RH<sub>n</sub>, n = 1 ... 6) with a selected current, adjusted by a potentiometer (P).  
165 The experiment was performed using an array of six independent sensors in the dark and under  
166 UV-light irradiation emitted by six OSV4YL5451B type diodes from *Opto-Supply*, China. Each  
167 diode was mounted above the sensor at the same distance, and the optical power irradiating the  
168 gas sensing layer was similar for each sensor.

169 The relative humidity and temperature inside the gas chamber was monitored during the  
170 experiment with a HIH 4000-002 humidity sensor from *Honeywell*, USA, and a LM35DZ  
171 temperature sensor from *Texas Instruments*, USA. The stability of the relative humidity  
172 ( $28\% \pm 5\%$ ) and temperature ( $40^{\circ}\text{C} \pm 1^{\circ}\text{C}$ ) were recorded.

### 173 **3. Results and discussion**

174 Firstly, an experimental study was performed to find the most suitable operating temperatures  
175 of the sensors that secured the best responses to exhaled breath samples. It was found that each  
176 sensor has a range of operating temperatures, usually between 90°C and 120°C for pristine WO<sub>3</sub>,  
177 Pt/WO<sub>3</sub> and Au/Pt/WO<sub>3</sub> sensors (Subset #1), and between 140°C and 200°C for Au/WO<sub>3</sub>,  
178 Ni/WO<sub>3</sub> and Fe/WO<sub>3</sub> sensors (Subset #2). We selected temperature ranges to include the  
179 optimal operating temperature for both sensor batches when exposed to breath samples.

180 Figure 6 shows the sensors' responses towards two successive breath exposures in the dark  
181 (blue curves) and under UV-light irradiation (red curves); the sensors from Subset #1 operated



182 at 100 °C (Fig. 6.a, Fig. 6.b, Fig. 6.c), and the sensors from Subset #2 at 160 °C (Fig. 6.d,  
183 Fig. 6.e and Fig. 6.f). Importantly, it can be seen that the sensors' responses became relatively  
184 more intense under UV-light irradiation than in the dark. This effect can be measured by a  
185 quotient  $Q$  of two conductances:

$$186 \quad Q = \frac{G_{F_{UV}}}{G_{F_{dark}}} \times 100\% \quad (1)$$

187 where:

- 188 •  $G_{F_{UV}}$  – conductance observed after breath exposure under UV-light at the final  
189 stage of the experiment,
- 190 •  $G_{F_{dark}}$  – conductance observed after breath exposure in the dark at the final stage of  
191 the experiment.

192 The quotient  $Q$  reached at least 150%. For the pristine  $WO_3$  NW sensor, it reached  $Q = 323\%$ .  
193 This result is associated with the photocatalytic reactions taking place in the sensing film and  
194 with decomposition of the breath VOCs that are then adsorbed by the sensing material  
195 (Trawka et al., 2016). When the photons' energy overtakes the energy band gap  $E_g$  of the  
196 semiconductor, a generated electron ( $e^-$ ) in the valence band is excited into the conduction band,  
197 leaving a positive hole ( $h^+$ ) in the valence band (Wu et al., 2015). The energy gap of  $WO_3$  is  
198  $E_g \approx 2.8$  eV, whereas the UV LEDs' wavelength is 394 nm, corresponding to a photon energy  
199 of 3.15 eV. As a photon's energy emitted from the UV LEDs is higher than the energy gap for  
200  $WO_3$  material, the sensor's conductance under UV-light irradiation should depend on the  
201 interband transitions (Giberti et al., 2012).

202 When the sensors operated under UV-light irradiation, their responses were repeatable and their  
203 recovery time was relatively short (Fig. 6). When the sensors operated under dark conditions,  
204 their responses were much longer and exceeded the observation time. We can claim that the use

205 of UV-light irradiation accelerated the desorption rate of the VOCs adsorbed by the sensing  
206 film before we switched to only the laboratory air. At the same time, UV-light quickened the  
207 saturation of the investigated sensors when exposed to VOCs.

208 Figure 7 displays the responses to breath exposure of three investigated sensors operating at  
209 selected temperatures. The presented data proves that under UV-light irradiation, the sensors  
210 provide more repeatable responses and with more intense relative changes of conductance as  
211 compared to their operation under dark conditions. This effect may be explained by intensified  
212 desorption in the presence of UV light which accelerates cleansing of the sensors after breath  
213 exposure. We have noticed that an increase of the sensor's operating temperature quickened its  
214 response but decreased its relative changes of conductance. Thus, for the pristine  $\text{WO}_3$  NW  
215 sensor, the UV/dark ratio (*see* Eq. 1) increased from 342% at 90 °C to 419% at 110 °C (when  
216 the sensor had not reached saturation during the experiment). At an operating temperature of  
217 120 °C, the sensor response in the dark (blue curve) was more intense than at lower  
218 temperatures, and therefore the UV/dark ratio of conductances decreased to 212% (Fig. 7.a,  
219 Fig. 7.b and Fig. 7.c). In the case of the Au/Pt/ $\text{WO}_3$  sensor, an operating temperature of 90 °C  
220 was too low to observe saturation or full recovery during the time of the experiment. The sensor  
221 started to saturate at a temperature of 110 °C both in the dark and under UV-light operation.  
222 UV-light irradiation assured a faster response, requiring only a few minutes, when compared to  
223 dark conditions, requiring about 30 min (Fig. 7.d, Fig. 7.e). For this sensor, again, the operating  
224 temperature of 120 °C assured more intense relative changes of conductance under dark  
225 conditions than at lower temperatures (Fig. 7.f). This is also observed for the Au/ $\text{WO}_3$  sensor  
226 at different operating temperatures. This sensor (Subset #2), showed that at an operating  
227 temperature of 140 °C, saturation cannot be achieved in the dark nor under UV-light (Fig. 7.g).  
228 Full saturation at an operating temperature of 180°C is reached after about 30 min of breath  
229 exposure in the dark and after about 15 min under UV-light (Fig. 7.h). As a consequence,



230 the coefficient  $Q$  decreased from 333% at 180 °C to 181% at 200 °C (Fig. 7.i). These results  
231 suggest that the presence of metal NPs on WO<sub>3</sub> NW surfaces could seriously improve the  
232 sensor's sensitivity to exhaled breath exposure, while reducing its optimal operating  
233 temperature.

234 Based on the time of response, operating temperature of the investigated sensors and relative  
235 change of DC resistance, we may determine their sensitivity to the exhaled breath. Sensitivity  
236  $S$  can be defined as a relative change of conductance  $G_F$  measured at the end of observation  
237 time (final conductance) in the ambient atmosphere of the exhaled breath and under dark  
238 conditions or UV-light irradiation (by using the index "dark or UV") and referenced to  
239  $G$  measured in the ambient atmosphere of laboratory air:

$$240 \quad S = \frac{G_{F(\text{dark or UV})} - G_0(\text{dark or UV})}{G_{(\text{dark or UV})}} \times 100\% \quad (2)$$

241  
242 All six sensors exhibited greater sensitivity when measured under UV-light irradiation at the  
243 investigated operating temperatures. Subset #1 of the sensors (pristine WO<sub>3</sub>, Pt/WO<sub>3</sub> and  
244 Au/Pt/WO<sub>3</sub>) reached higher sensitivities towards breath exposures at 100 °C both in the dark  
245 and under UV-light irradiation (Fig. 8.a, Fig. 8.b), which drastically decreased at 110 °C and  
246 further at 120 °C under UV-light irradiation. In the case of the sensors from Subset #2 (Au/WO<sub>3</sub>,  
247 Ni/WO<sub>3</sub> and Fe/WO<sub>3</sub>), their sensitivity changed slightly at the considered operating  
248 temperatures and in the dark (Fig. 8.c), while under UV-light irradiation, the changes were  
249 much more intense and the greatest sensitivity was observed at 160 °C (Fig. 8.d). The most  
250 significant difference between the sensitivity in the dark and under UV-light irradiation was  
251 found for the Au/WO<sub>3</sub> sensor, which increased from 88.9 % to 216.9% at 160 °C.

252 The reported results mean that a proper combination of the sensors' heating and UV-irradiation  
253 may play a crucial role in enhancing MOS WO<sub>3</sub> sensors' sensitivity towards the detection of

254 the VOC's in the exhaled breath. Their functionalisation by metal-doped nanoparticles is also  
255 important to determine the sensors' optimal operating temperature, together with the sensors'  
256 sensitivity and selectivity.

#### 257 **4. Conclusions**

258 Our experimental study presents the first ever report of UV-irradiation combined with a  
259 selection of the sensors' operating temperatures to enhance exhaled breath detection by WO<sub>3</sub>  
260 NW sensors decorated by selected metal dopants. The study was performed on both pristine  
261 and NP-doped WO<sub>3</sub> NWs grown by AACVD on alumina substrates and characterised by AFM,  
262 SEM, TEM and EDX-ray. All sensors clearly responded to the exhaled breath, both in the dark  
263 and under UV-light irradiation. In addition, their responses were repeatable and determined by  
264 their operating temperatures. The experimental results revealed that the most sensitive sensor  
265 towards the exhaled breath samples was the Au-doped WO<sub>3</sub> NWs operating at 160 °C.  
266 It reached a sensitivity as high as  $S = 216.9\%$  under UV-light irradiation. These promising  
267 results may be a way for further development of low-cost, low-power consumption and highly  
268 sensitive gas sensors for medical applications.

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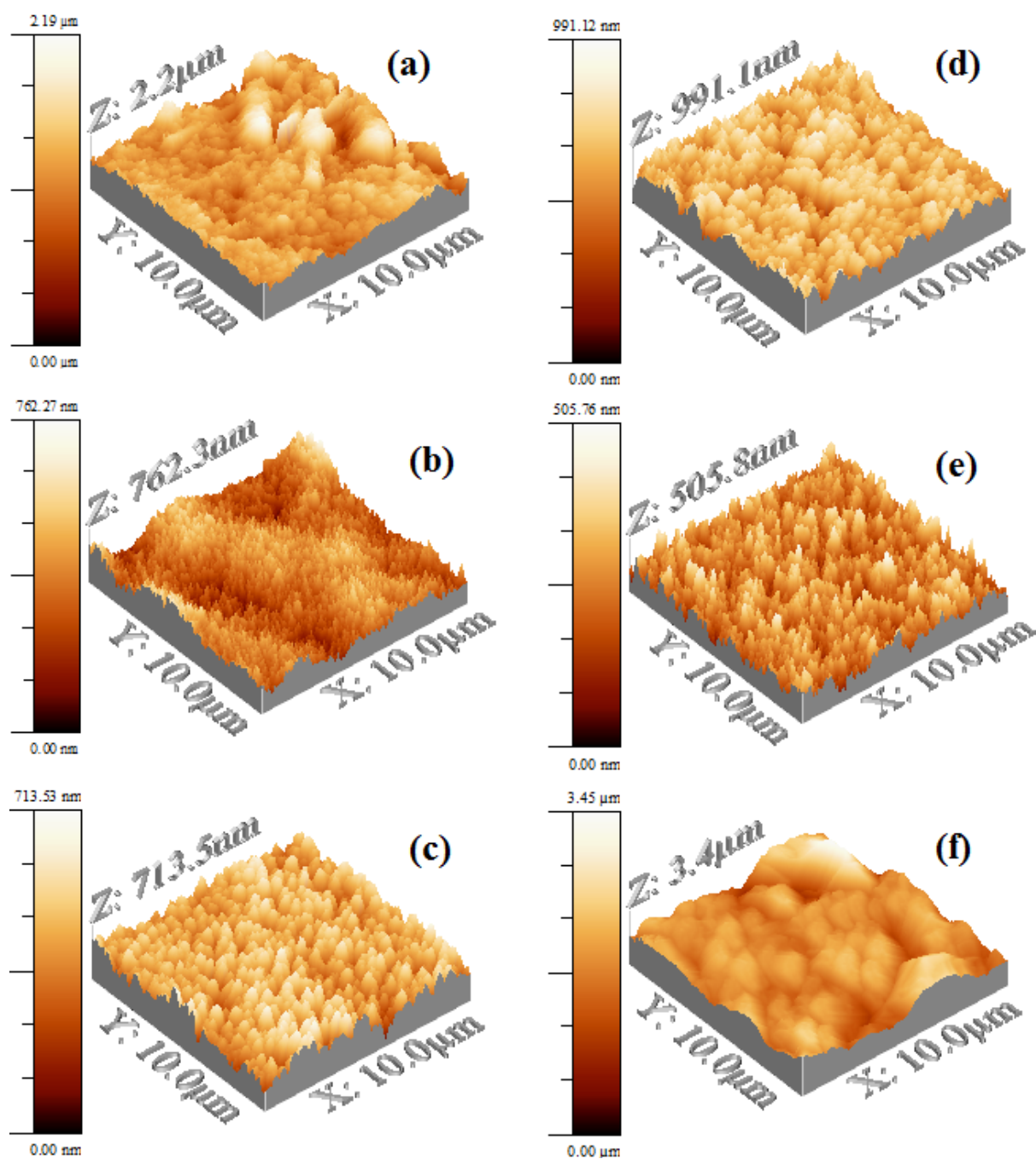
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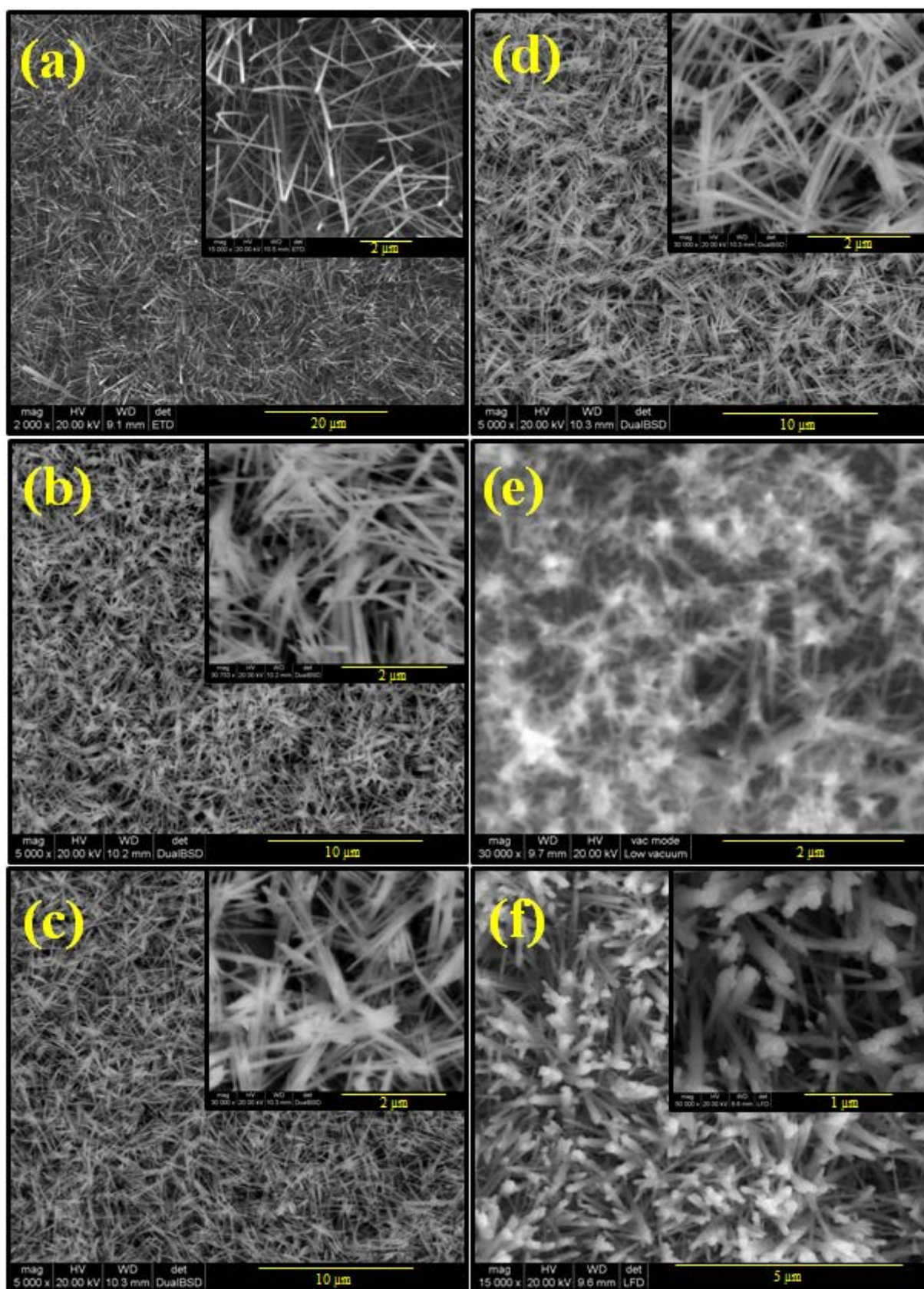
## Highlights

- AACVD was carried out to produce pristine and differently functionalised WO<sub>3</sub>
- The grown sensors were characterised with AFM, SEM, TEM and EDX-ray
- UV-light irradiation enhanced the sensors' responses towards breath exposure
- The most sensitive sensor for breath was the Au-doped WO<sub>3</sub> and operating at 160 °C

**Figure 1** AFM topographies of the sensors' surfaces of: (a) pristine  $\text{WO}_3$ ; (b)  $\text{Pt}/\text{WO}_3$ ; (c)  $\text{Au}/\text{Pt}/\text{WO}_3$ ; (d)  $\text{Au}/\text{WO}_3$ ; (e)  $\text{Ni}/\text{WO}_3$ ; (f)  $\text{Fe}/\text{WO}_3$ .

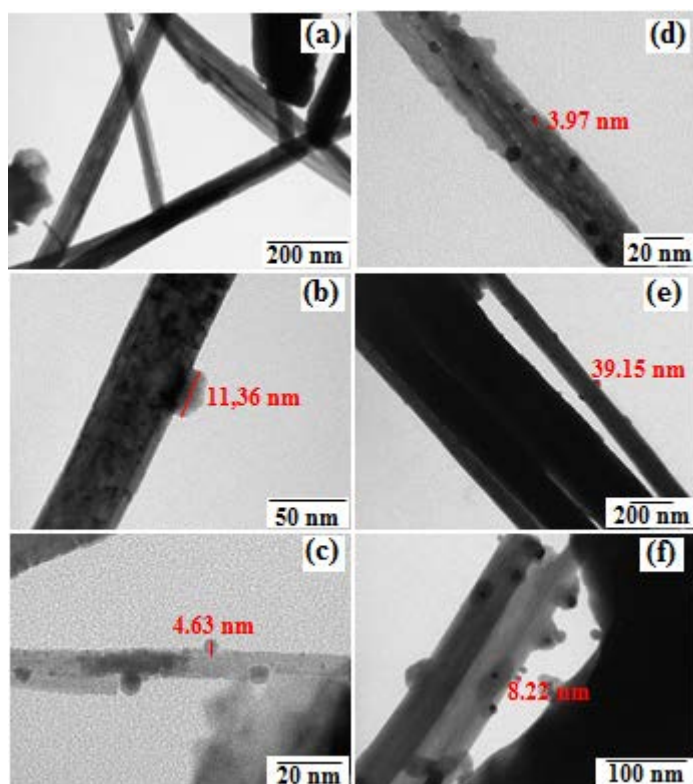


**Figure 2** Typical SEM images of sensing areas of: (a) pristine  $\text{WO}_3$ ; (b)  $\text{Pt}/\text{WO}_3$ ; (c)  $\text{Au}/\text{Pt}/\text{WO}_3$ ; (d)  $\text{Au}/\text{WO}_3$ ; (e)  $\text{Ni}/\text{WO}_3$ ; (f)  $\text{Fe}/\text{WO}_3$ .

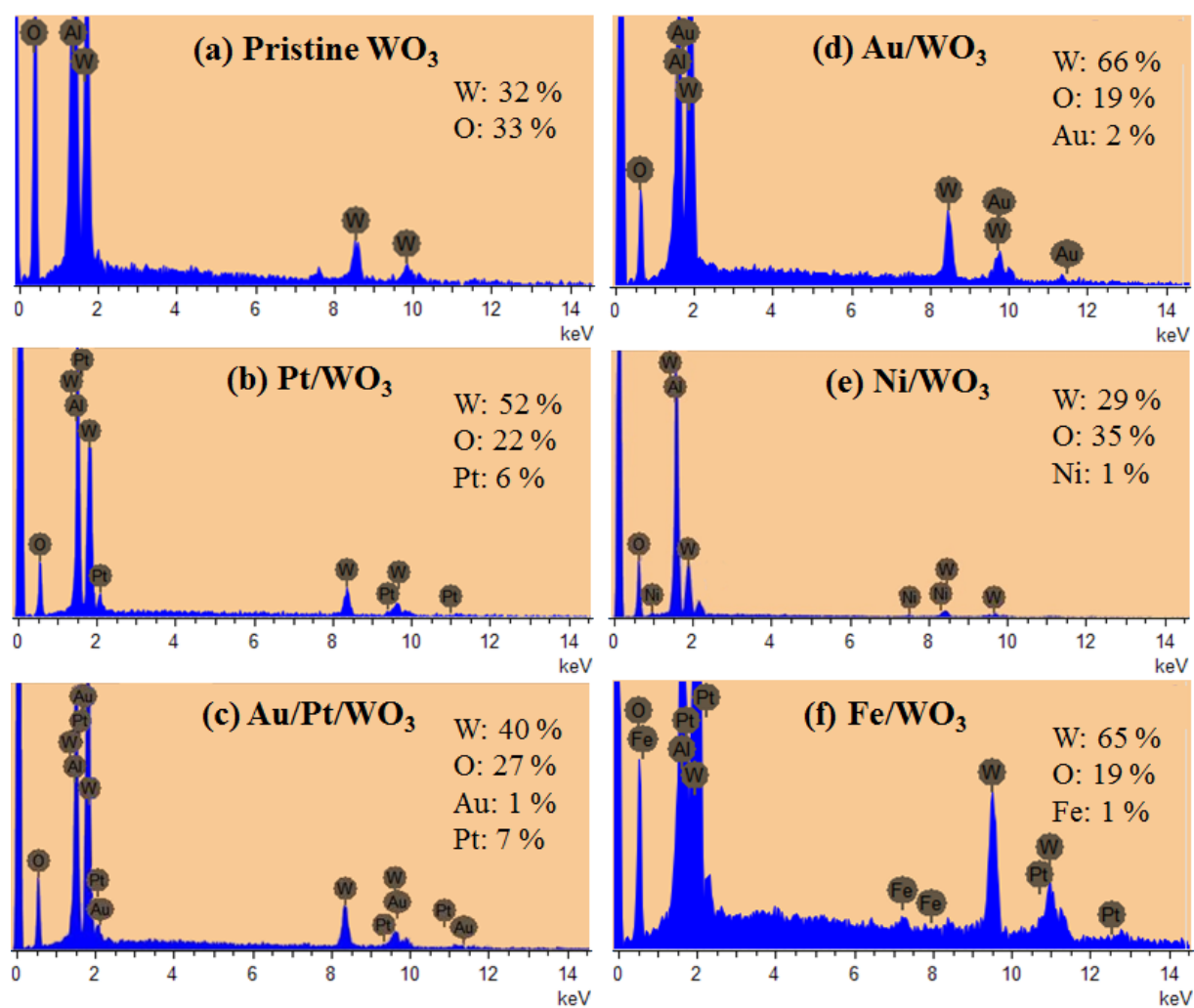




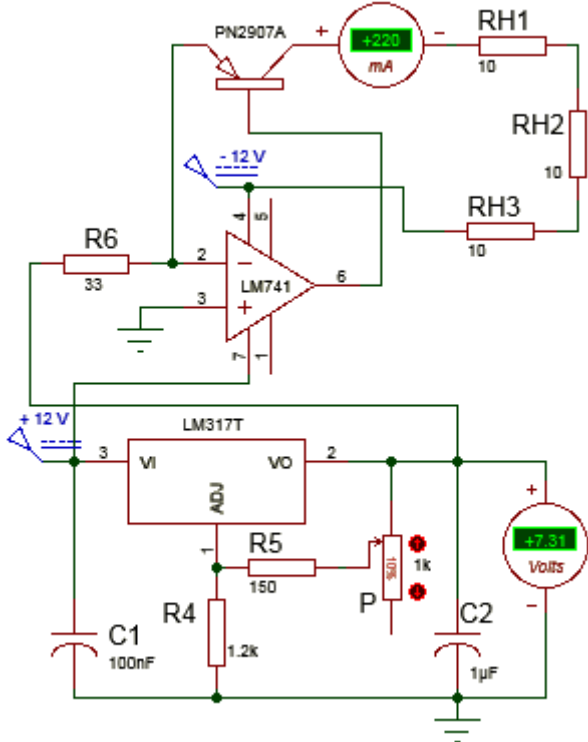
**Figure 3** TEM images of the sensitive films of: (a) pristine  $\text{WO}_3$ ; (b)  $\text{Pt}/\text{WO}_3$ ; (c)  $\text{Au}/\text{Pt}/\text{WO}_3$ ; (d)  $\text{Au}/\text{WO}_3$ ; (e)  $\text{Ni}/\text{WO}_3$ ; (f)  $\text{Fe}/\text{WO}_3$ .



**Figure 4** EDX-ray spectrum of the six sensors: **(a)** pristine  $\text{WO}_3$ ; **(b)**  $\text{Pt}/\text{WO}_3$ ; **(c)**  $\text{Au}/\text{Pt}/\text{WO}_3$ ; **(d)**  $\text{Au}/\text{WO}_3$ ; **(e)**  $\text{Ni}/\text{WO}_3$ ; **(f)**  $\text{Fe}/\text{WO}_3$ .

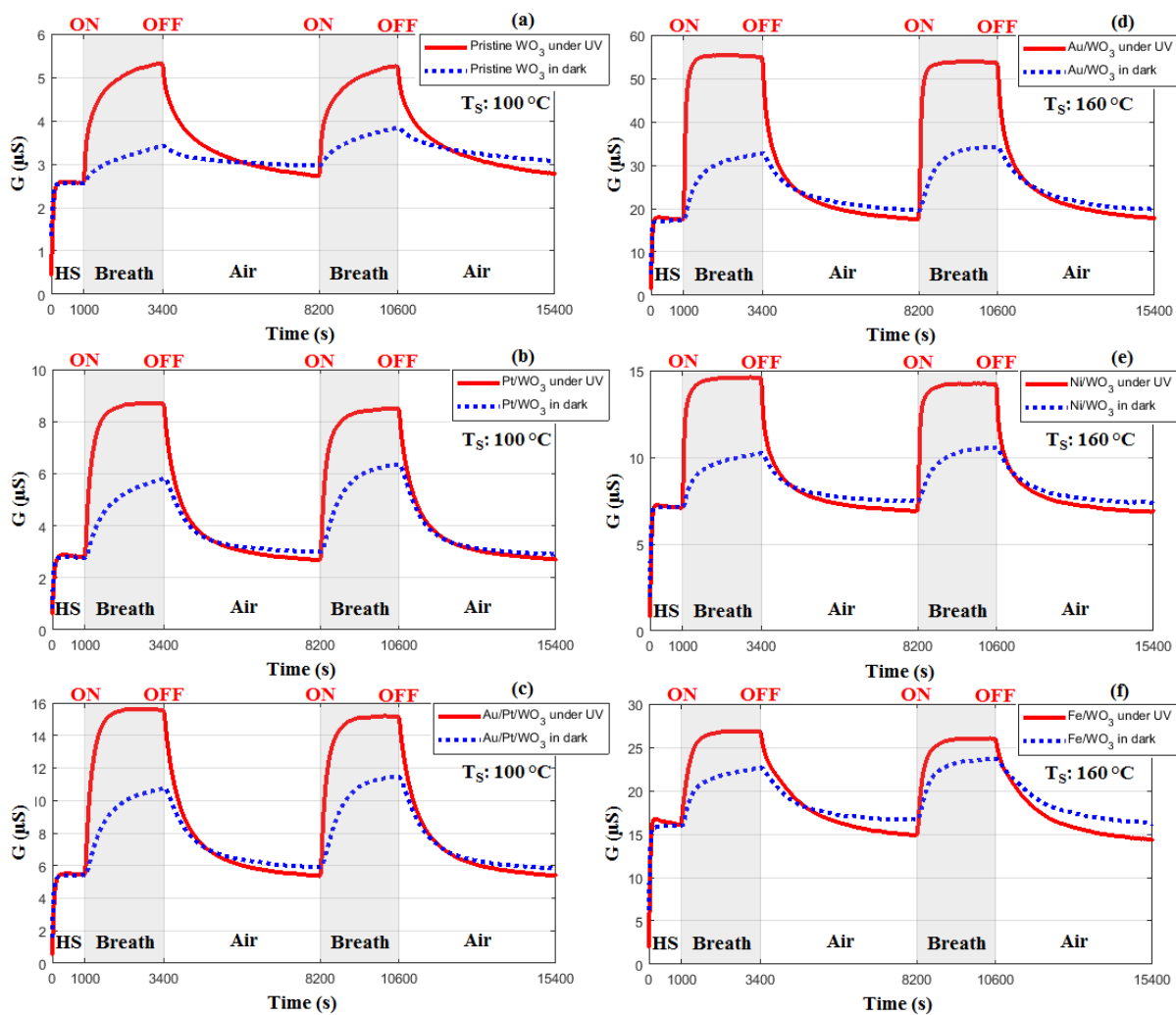


**Figure 5** Electronic conditioning circuit for monitoring the current of three sensors' heaters connected in series.

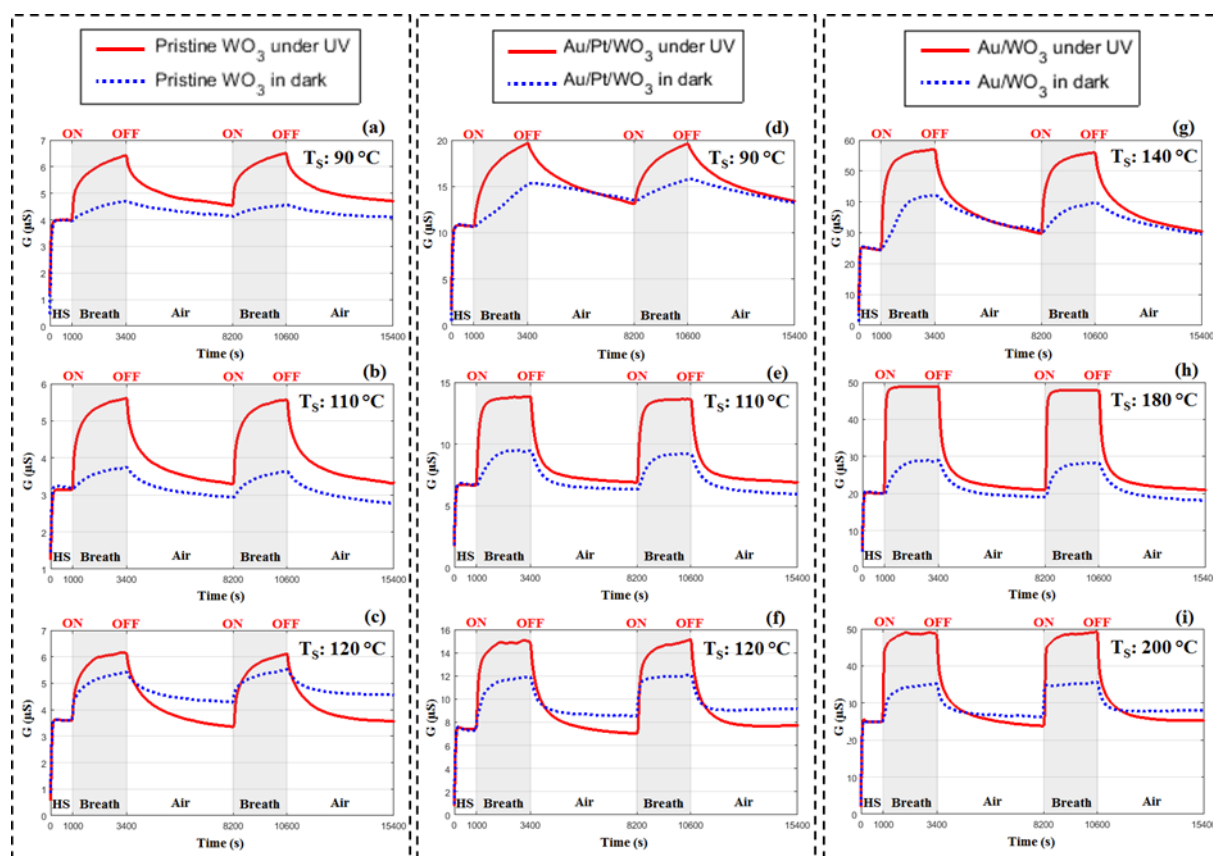




**Figure 6** Sensors responses towards two repeated breath exposures in the dark (blue curves) and under UV-light illumination (red curves) for: (a) Pristine  $\text{WO}_3$ ; (b)  $\text{Pt}/\text{WO}_3$ ; (c)  $\text{Au}/\text{Pt}/\text{WO}_3$ ; (d)  $\text{Au}/\text{WO}_3$ ; (e)  $\text{Ni}/\text{WO}_3$ ; (f)  $\text{Fe}/\text{WO}_3$ . Sensors (a) to (c) were operated at  $100^\circ\text{C}$ , and sensors (d) to (f) at  $160^\circ\text{C}$ .



**Figure 7** Sensors responses towards two repeated breath exposures in the dark (blue curves) and under UV-light illumination (red curves) for Pristine  $\text{WO}_3$  sensor operated at: (a)  $90^\circ\text{C}$ ; (b)  $110^\circ\text{C}$ ; (c)  $120^\circ\text{C}$ ;  $\text{Au/Pt/WO}_3$  sensor operated at: (d)  $90^\circ\text{C}$ , (e)  $110^\circ\text{C}$ ; (f)  $120^\circ\text{C}$ ;  $\text{Au/WO}_3$  sensor operated at: (g)  $140^\circ\text{C}$ ; (h)  $180^\circ\text{C}$ ; (i)  $200^\circ\text{C}$ .



**Figure 8** Sensors sensitivities in the presence of breath exposure at four different temperatures for pristine  $\text{WO}_3$ ,  $\text{Pt}/\text{WO}_3$ ,  $\text{Au}/\text{Pt}/\text{WO}_3$ : (a) in dark, (b) under UV irradiation; and  $\text{Au}/\text{WO}_3$ ,  $\text{Ni}/\text{WO}_3$ ,  $\text{Fe}/\text{WO}_3$ : (c) in dark, (d) under UV irradiation.

